## Improved 3D real-time MRI with Stack-of-Spiral (SOSP) trajectory and variable density randomized encoding of speech production

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Target Audience: Linguists; MR engineers who focus on non-Cartesian and dynamic imaging.

**Purpose:** To develop and evaluate an improved sampling strategy for three-dimensional (3D) real-time (RT) MRI of the entire vocal tract, with high spatio-temporal resolution during natural speech. RT-MRI has emerged as an efficient tool to understand the complex spatio-temporal  $\leq$  coordination of vocal tract articulators during speech production<sup>1</sup>. Speech RT-MRI faces fundamental trade-offs between spatial resolution, temporal resolution, spatial coverage, signal-to-noise ratio (SNR), and artifacts, which are common to all fast MRI. Since 2004 2D mid-sagittal RT-MRI has been extensively applied to speech production research<sup>2</sup> and is considered to be a standard and mature method. Recently, 3D RT-MRI has provided an opportunity to study the entire vocal tract volume in montion<sup>3</sup>. Lim et al.<sup>4</sup> demonstrated the feasibility of 3D RT-MRI of natural speech, with full vocal tract coverage, 2.4×2.4×5.8 mm<sup>3</sup> spatial resolution and 61ms  $_{\leq}$  temporal resolution. Inspired by this study, we explore and evaluate improved (k,t) data sampling strategies and constrained reconstruction options for 3D RT-MRI with improved spatio-temporal resolution during natural speech tasks.

**Methods:** Data sampling and reconstruction Figure 1 illustrates a proposed sampling strategy compared to the prior work of Lim et al.<sup>4</sup>. During each TR, we acquire one spiral arm in the  $k_x - k_y$  plane to achieve 13-fold acceleration. A pseudo-golden angle increment is used in the  $k_x - k_y$  plane, and Cartesian sampling is employed along the  $k_z$  direction. In Lim's method<sup>4</sup>,  $k_z$  steps are sampled in a linear order. Spiral patterns are tilted with a golden-angle increment after 12 phase encodings (corresponding to full  $k_z$  sampling). In the proposed method, we applied a rotated a golden-angle in the  $k_x - k_y$  plane for each phase encoding step.  $k_z$  was sampled randomly



**Figure 1: Sampling Patterns.**  $k_z$  vs. time plots illustrate sampling strategies of the original method from Lim et al<sup>4</sup> (top) and the proposed method (bottom). Each dot represents one spiral arm in the  $k_x$  -  $k_y$  plane; color represents its initial angle as shown by the color map shown at the right.

according to a variable density function. Image reconstruction was performed by solving the following constrained optimization:

$$\arg\min_{f(r,t)} \|A(f) - \boldsymbol{b}\|_{2}^{2} + \lambda_{1} \|TV(f)\|_{1} + \lambda_{2} \|D_{t}(f)\|_{1}$$

where  $f(\mathbf{r}, t)$  is the dynamic image time series to be reconstructed, and the vector  $\mathbf{r} \in (x, y, z)$  represents image domain spatial coordinates.  $\mathbf{b}$  is multi-coil k-t space measurement data. A refers to coil sensitivity encoding as well as Fourier operator along each time frame in 3D volume. Isotropic total variation (TV) and first-order finite difference  $(D_t)$  constraints were applied along spatial and temporal dimensions, respectively. Reconstruction was implemented in MATLAB and using the Berkeley Advanced Reconstruction Toolbox<sup>5</sup>. The regularization parameters  $\lambda_1$  and  $\lambda_2$  were chosen visually based on the image quality in sagittal views and time-intensity plots. We chose  $\lambda_1 = 0.008$ ,  $\lambda_2 = 0.03$ .

<u>In-vivo</u> Experiments Experiments were performed on a 1.5 T Signa Excite HD scanner (GE Healthcare, Waukesha, WI), using the real-time imaging platform (RT-Hawk, Heart Vista Inc, Los Altos, CA). Experiments used the body coil for RF transmission and a custom eight-channel upper airway coil for signal reception. Two healthy adult volunteers were scanned. Speaker 1 (male native Chinese speaker, English as a second language) was scanned while reading the English stimuli: "/loo/-/lee/-/la/-/za/-/na/-/za/" repeated twice at a natural rate. Speaker 2 (male American English speaker) was scanned with a 3D sequence using the original and the proposed sampling patterns, as well as 2D three-slice sequences as reference<sup>6</sup>. The stimuli for Speaker 2 include 4 sentences and were each spoken twice, once at a natural rate and once at a speaking rate of approximately 1.5× the initial rate. All stimuli were read in the scanner using a mirror projector setup used for display<sup>7</sup>.

**Results: Figure 2** shows the stimuli results for the original 3D and proposed 3D methods, along with the interleaved 2D multi-slice method (reference). Fast lip opening and closing in a speeded rate (blue dotted box) can be better captured using proposed method. Images are significantly blurred for tongue body movements in the original method (pink, yellow and green arrows).

**Discussion:** In this study, four other sampling schemes were also designed, which allowed pairwise comparisons for a single change of sampling strategy. Due to the space constraints, they are not shown here. Our proposed method, the randomized variable density stack-of-spiral sampling, enables retrospective selection of temporal resolution. We found that better temporal resolution enables capturing fast movements of certain articulators, while a relatively high SNR can be preserved with adequate temporal resolution.

**Conclusion:** We have demonstrated 3D RT-MRI of the vocal tract with improved spatio-temporal resolution achieved by using randomized variable density stack-of-spiral sampling, combined with a spatially and temporally constrained reconstruction. Improved capture and visualization of several speech tasks is achieved notably during fast lip and tongue movements.

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**Figure 2. Stimuli results.** A. 3D original, B. 3D proposed and C. 2D multi-slice method. Top row for A-C: a. sagittal reference and b. time intensity plots during two repeated trials at normal and speeded rates. Gray arrows 1-6 indicate specific frames below. Second row for A-C: Six representative frames in c. sagittal and d. axial views that capture /a/, /æ/, /i/ vowels.

References: [1] Lingala, et al., JMRI (2016) [2] Niebergall, et al., MRM (2013) [3] Burdumy, et al., JMRI (2017) [4] Lim, et al., MRM (2019) [5] Uecker, et al., Proc. Intl. Soc. Mag. Reson. Med. (2015) [6] Kim, et al., JMRI (2012) [7] Lingala, et al., INTERSPEECH (2016)